

Dosimetry Measurement of Medical Linear Accelerator and Assessment the Authentication it with Machine Records

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Abstract

Absolute dosimetry for photon energies of a medical linear accelerator were obtained for 1 D water phantom and solid water phantom with farmer chamber (FC 65-P) for 6 MV and 15 MV photon beam generated from medical linear accelerator (Clinac iX, Varian) of Institute of Nuclear Medical Physics (INMP), Bangladesh atomic energy commission. The machine was tuned to deliver 1 cGy/MU at SSD technique at Dmax for all the available photon energies. The measurements were done using the Source to Surface Distance (SSD) technique at 10 cm depth with 10 cm² × 10 cm² field size. Beam quality index were measured for two photon energies using the Tissue Phantom Ratio TPR_{20,10} and correction factor K_Q values are taken from IAEA TRS-398. The electrometer readings were corrected for temperature-pressure, polarity and recombination effect. The corrected meter readings were multiplied with the calibration factor provided by the Secondary Standard Dosimetry Laboratory (SSDL) and also with K_Q values. For 1D water phantom, a variation with machine data was obtained as 0.9% and 1.77% for 6 MV and 15 MV photon beam respectively. For solid water phantom, a variation with machine data was obtained as 0.3% and 0.35% for 6 MV and 15 MV photon beam respectively. The beam quality parameters of the available photon beams were found to be Varian acceptance tolerance and also compatible with the IAEA TRS 398 recommendations.

Keywords: Absolute dosimetry; Medical linac; Source to surface distance

Introduction

Cancer is increasing significantly day by day in Bangladesh. According to World Health Organization (WHO) report, there are fifteen lakh cancer patients in Bangladesh and each year two lakh patients are newly added. One and half lakh dies every year. In Bangladesh there is significant shortage of qualified medical physicist and the scope of medical physics education is rare. For diagnosis, treatment and management of cancer patients, many of these patients go to neighboring countries for these purposes, incurring huge monetary loss to the country. Medical Physics is concerned with the applications of physics and nuclear physics concepts and techniques to the diagnosis and treatment of human disease. medical physicists work with physicians, technologists, nurses and other stuffs assisting patients who need nuclear imaging technology and cancer treatment in medicine. In addition, medical physicists focus on radiation protection, research, teaching and consulting etc.

Case

The absorbed dose to water is the main quantity used in radiation therapy. The advantages obtained from the use of water include reduced uncertainty, a more robust system of primary standards and the use of a simple formalism [1]. In this paper the absolute dose of the photon beam of a medical linac (varian clinac iX) was analyzed using 1D water phantom and solid phantom and then compared these measurement with machine data.

Materials and Methods

The absorbed dose to water at any reference depth, Zref in water: [2]

$$D_{w,Q} = M_Q N_{D,w,Q_0} k_{Q,Q_0} \text{-----(1)}$$

For Corrected dosimeter reading at voltage V1

$$M_Q = M_1 \times K_{T,P} \times K_e \times K_{Pol} \times K_S \quad (2)$$

The value of beam quality correcting factor, was corrected for the effect of the differences between the reference beam quality Q_0 and the actual user quality Q . The beam Quality Q of a megavoltage photon beam is specified with either with tissue-phantom ratio or with the Percentage Depth Dose PDD. $TPR_{20,10}$ is defined as the ratio of doses on the beam central axis at depths of $z = 20$ cm and $z = 10$ cm in water obtained at an SAD of 100 cm and a field size of $10 \text{ cm}^2 \times 10 \text{ cm}^2$. $TPR_{20,10}$ is independent of electron contamination of the incident photon beam.

Results and Discussion

Absolute dosimetry using 1D water phantom measurement

The measurements were conducted using varian clinac ix (manufacture: varian medical system, USA) (varian oncology) at the institute of nuclear medical physics, Bangladesh atomic energy commission [3,4].

It has two photon energies 6 MV and 15 MV and five electron energies (e.g. 6 MeV, 9 MeV, 12 MeV, 15 MeV and 18 MeV). Absolute dosimetry for 6 MV and 15 MV photon energies were measured by using a 1D water phantom with Farmer Chamber (FC 65-P) for 6MV and 15MV. For this study, 1D phantom, ionization chambers, and electrometers are used.

The ionization chamber is the most practical and most widely used type of dosimeter for accurate measurement of machine output in radiotherapy [5].

The ionization chamber is put in a water phantom, and is connected with a electrometer. The measurements were done using the Source to Surface Distance (SSD) technique at 10 cm depth with $10 \text{ cm}^2 \times 10 \text{ cm}^2$ field size.

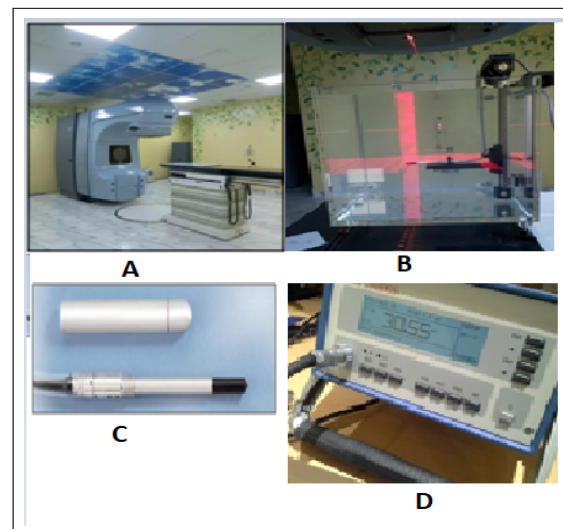


Figure 1: Experimental set up for absolute dosimetry measurement using 1d water phantom. A) Medical Linac; B) 1D Stand alone water phantom; C) Ionization Chamber: FC 65P; D) Electrometer.

Figure 1 shows some experimental set up for the measurement of absorbed dose to water. Temperature and pressure was found to be $T=18.9^\circ \text{C}$ and $P=1009 \text{ hpa}$. T_0 and P_0 from the standards laboratory was $T_0=20^\circ \text{C}$ and $P_0=1013.25 \text{ hpa}$. The machine was irradiated with a voltage of $V=+300 \text{ V}$. For pulsed beam we used the ratio $V1/V2=3$. We used the calculation for 100 Monitor Unit (MU) with dose rate 400. The chamber calibration factor, $N_{D,w}=4.789 \text{ Gy/C} \times 10^7 \text{ Gy/C}$ was taken from chamber calibration certificate. To find out $TPR_{20,10}$ for 6MV and 15 MV, the ionization chamber was placed at depth of 20 cm with SSD=80 cm, field size $10 \text{ cm}^2 \times 10 \text{ cm}^2$ and data was taken. Then the ionization chamber was placed at depth of 10 cm with SSD=90 cm, field size $10 \text{ cm}^2 \times 10 \text{ cm}^2$ and data were taken. Table 1 shows the data for beam quality correction factor $TPR_{20,10}$ (Table 1).

Energy	Depth=20 cm, SSD=80 cm		Depth=10 cm, SSD=90 cm	
	Reading (nC)	Mean (nC)	Reading (nC)	Mean (nC)
6 MV	11.42	11.415	17.1	17.1
	11.41		17.1	
15 MV	15.27	15.275	20.13	20.13
	15.28		20.13	

Table 1: Determination of the value of $TPR_{20,10}$ for 1D water phantom.

For 6 MV photon beam, $TPR_{20,10}$ was found 0.667. Using that value K_Q was found to be 0.993 from IAEA TRS-398 [2]. For 15 MV photon beam, $TPR_{20,10}$ was found 0.7588 and K_Q was found to be 0.976 To correct the signal some factors are involved. The ionization chamber was set for SSD=100 cm, at 10 cm depth with field size $10\text{ cm}^2 \times 10\text{ cm}^2$ and data was taken. To correct the signal some factors are involved. Table 2 shows data for determination of M_+ , M_- and M_2 . M_1 was same as M_+ .

Energy	M+ (+300 V)		M-(-300V)		M2(+100V)	
	Reading (nC)	Mean (nC)	Reading (nC)	Mean (nC)	Reading (nC)	Mean (nC)
6MV	14.3	14.3	14.3	14.305	14.17	14.17
	14.3		14.31		14.17	
15MV	16.76	16.76	16.77	16.77	16.5	16.505
	16.76		16.77		16.51	

Table 2: Determination of M_+ , M_- and M_2 for 1D water phantom.

Now the absorbed dose to water for 6 MV photon beam at reference depth, Z_{ref} using equation (2) becomes

$$D_{w,Q}(z_{ref}) = M_1 \times K_{T,P} \times K_e \times K_{Pol} \times K_S \times N_{D,w} \times K_Q = 0.6833 \text{ cGy} / MU$$

Percentage Depth Dose, PDD for 6 MV photon beam = 67.7, was taken from INMP medical linac data profile which was also similar as other institute [6]. Using this value we can determine Absorbed dose to water for 6 MV photon beam at the depth of dose maximum, Z_{max} by using [2]

$$D_{w,Q}(z_{max}) = 100 \frac{D_{w,Q}(z_{ref})}{P_{DD}(z_{ref})} = 100 \times \frac{0.6833}{67.7} = 1.009 \text{ cGy} / MU$$

Absorbed dose to water for 15 MV photon beam at reference depth, z_{ref} using equation (2)

$$D_{w,Q}(z_{ref}) = M_1 \times K_{T,P} \times K_e \times K_{Pol} \times K_S \times N_{D,w} \times K_Q = 0.7816 \text{ cGy} / MU$$

Percentage Depth Dose, PDD for 15 MV photon beam=76.8, was taken from INMP medical linac data profile which was also similar as other institute [6]. Absorbed dose to water for 15 MV photon beam at the depth of dose maximum, Z_{max} [2].

$$D_{w,Q}(z_{max}) = 100 \frac{D_{w,Q}(z_{ref})}{P_{DD}(z_{ref})} = 100 \times \frac{0.7816}{76.8} = 1.0177 \text{ cGy} / MU$$

Absolute dosimetry using solid water phantom measurement

For the measurement of absorbed to water in case of solid water phantom, temperature and pressure was found to be $T=19.50^\circ\text{C}$ and $P=1000.8\text{ hpa}$. T_0 and P_0 from the standards laboratory was $T_0=20^\circ\text{C}$ and $P_0=1013\text{ hpa}$. Table 3 shows the data for beam quality correction factor $TPR_{20,10}$ (Table 3).

Energy	Depth=20 cm, SSD=80 cm		Depth=10 cm, SSD=90 cm	
	Reading (nC)	Mean (nC)	Reading (nC)	Mean (nC)
6 MV	11.07	11.075	16.77	16.77
	11.08		16.77	
15 MV	14.81	14.815	19.67	19.67
	14.82		19.67	

Table 3: Determination of the value of $TPR_{20,10}$ for solid water phantom.

For 6 MV photon beam, $TPR_{20,10}$ was found . Using that value K_Q was found to be 0.994 from IAEA TRS-398 [2]. For 15 MV photon beam, $TPR_{20,10}$ was found and value of K_Q was found to be 0.978. Table 4 shows data for determination of M_+ , M_- and M_2 . M_1 was same as M_+ (Table 4).

Energy	M+ (+300V)		M-(-300V)		M2(+100V)	
	Reading (nC)	Mean (nC)	Reading (nC)	Mean (nC)	Reading (nC)	Mean (nC)
6 MV	13.99	13.985	14	14	13.88	13.88
	13.98		14		13.88	
15 MV	16.33	16.33	16.33	16.33	16.08	16.075
	16.33		16.33		16.07	

Table 4: Determination of M_+ , M_- and M_2 for solid water phantom.

Now the absorbed dose to water for 6 MV photon beam at reference depth, Z_{ref} using equation (2) becomes

$$D_{w,Q}(z_{ref}) = M_1 \times K_{T,P} \times K_e \times K_{Pol} \times K_S \times N_{D,w} \times K_Q$$

$$= 0.697 \text{ cGy} / \text{MU}$$

Percentage Depth Dose, PDD for 6 MV photon beam=67.7, was taken from INMP medical linac data profile which was also similar as other institute [6]. Using this value we can determine absorbed dose to water for 6 MV photon beam at the depth of dose maximum, Z_{max} by using [2].

$$D_{w,Q}(z_{max}) = 100 \frac{D_{w,Q}(z_{ref})}{P_{DD}(z_{ref})} = 100 \times \frac{0.697}{67.7} = 1.003 \text{ cGy} / \text{MU}$$

Absorbed dose to water for 15 MV photon beam at reference depth, Z_{ref} using equation

(2)

$$D_{w,Q}(z_{ref}) = M_1 \times K_{T,P} \times K_e \times K_{Pol} \times K_S \times N_{D,w} \times K_Q$$

$$= 0.7707 \text{ cGy} / \text{MU}$$

Percentage Depth Dose, PDD for 15 MV photon beam=76.8, was taken from INMP medical linac data profile which was also similar as other institute [6]. Absorbed dose to water for 15 MV photon beam at the depth of dose maximum, Z_{max} [2].

$$D_{w,Q}(z_{max}) = 100 \frac{D_{w,Q}(z_{ref})}{P_{DD}(z_{ref})} = 100 \times \frac{0.7707}{76.8} = 1.0035 \text{ cGy} / \text{MU}$$

Assessment the authentication it with machine records

Table 5 shows the comparison of absorbed dose to water at the depth of dose maximum, Z_{max} for 1D water phantom and solid water phantom and shows the variations it with machine data for 6 MV and 15 MV photon beam.

Photon energy	Machine data	1D water phantom	Deviation	Solid water phantom	Deviation
6MV	1cGy/MU	1.009 cGy/MU	0.90%	1.003 cGy/MU	0.30%
15MV	1cGy/MU	1.0177 cGy/MU	1.77%	1.0035 cGy/MU	0.35%

Table 5: Absorbed dose (at the depth of dose maximum, Z_{max}) variation of 1 D water phantom and solid water phantom with the machine data.

Conclusion

Absolute dosimetry for photon energies was determined using the IAEA Technical Report Series (TRS-398). The machine was tuned to deliver 1cGy/MU at SSD technique at D_{max} for all the available photon energies and kept as a baseline. Beam quality index were measured for all the energies using the TPR_{20,10} and absolute dose determination were done at 10 cm depth using SSD technique. All the measurements were carried out using the IBA 1D water phantom and solid water phantom with farmer 0.65 cc (FC 65-P) chamber. The meter readings were corrected for temperature-pressure correction, polarity effect and recombination effect. The corrected meter readings were multiplied using the absolute dose to water calibration factor ($N_{D,w,Q}$) provided by the secondary standard dosimetry lab along with the appropriate K_Q according to the beam quality. Absorbed dose to water at reference depth (10 cm) for 1D water phantom for 6 MV and 15 MV photon beam was found to be 0.68 cGy/MU and 0.78 cGy/MU. Absorbed dose to water at the depth of dose maximum (Z_{max}) for 6 MV and 15 MV Photon Beam was found to be 1.009 cGy/MU and 1.0177 cGy/MU. For solid water phantom absorbed dose to water at reference depth (10 cm) for 6 MV and 15 MV photon beam was found to be 0.697 cGy/MU and 0.77 cGy/MU. Absorbed dose to water at the depth of dose maximum (Z_{max}) for 6 MV and 15 MV photon beam was found to be 1.003 cGy/MU and 1.0035 cGy/MU.

For 1 D water phantom, a variation with machine data was obtained as 0.9% and 1.77% for 6 MV and 15 MV photon beam respectively. For Solid Water phantom, a variation with machine data was obtained as 0.3% and 0.35% for 6 MV and 15 MV photon beam respectively. The beam quality parameters of the available photon beams were found to be Varian acceptance tolerance and also compatible with the IAEA TRS 398 recommendations.

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